

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

UNITED STATES PATENT APPLICATION

for

Apparatus for Generating Shock Waves

based on the prior application of the Swiss Patent Application:

Title: "Vorrichtung zur Erzeugung von Stosswellen"

Application Number: 2003 0299/03

Filing Date: 26. February 2003

Assignee

HMT High Medical Technologies AG
Kreuzlingerstrasse 5
CH-8574 Lengwil /Switzerland

Inventor - Assignor

Mr. Erwin Simnacher
In der Abtwiese 22
D-78479 Reichenau / Germany

Apparatus for Generating Shock Waves

BACKGROUND OF THE INVENTION

5

The invention relates to an apparatus for generating shock waves directed at an area of a human or animal body to be treated using piezoelectric fibers. The piezofibers integrated in a composite material are controlled for this, and together
10 with a control unit they form the shock-wave generating part.

Shock waves are used for different purposes in human and veterinary medicine. A medical use of these apparatuses in human medicine is lithotripsy, where the generated shock waves
15 are focused on internal objects to be destroyed, such as kidney stones. Further applications are, for instance, inducing of bone growth, treatment of orthopaedically painful diseases (epicondylitis, calcified shoulder) and treatment of nerves, muscles and other soft-tissue structures.

20

The generation of shock waves using piezoelectric ceramic elements is generally known, for instance from US 5,101,133. A multitude of piezoelectric ceramic elements are arranged on a spherical calotte and form an electro-acoustic transducer.

25

The arrangement of this multitude of piezoelectric ceramic elements of the known apparatus is very complex and costly as regards their production.

30

The piezoelectric ceramic elements are embedded in a casting compound of for instance an epoxy resin mixture. Since the radiating surface of the piezoelectric ceramic elements covers an area of several square millimeters up to some square centimeters, the deformation of the piezoelectric
35 ceramic elements leads to a high strain of the casting compound on the boundary layer to the ceramic elements.

40

Generally, the miniaturization of the structural shape of the shock-wave generating apparatus is aimed at. This aim is pursued in order to simplify the handling of the apparatuses, on the one hand, and to open up new applications, for instance for the treatment of salivary stones, on the other hand.

In addition, it is desirable to focus the shock waves on areas having a different geometry. Freely selectable geometric forms of the shock-wave generating systems are required for this. A high efficiency for special applications is reached in this way, for instance for the treatment of long bone-fissures or cellulites.

In view of the above embodiment the invention is based on the task to provide an apparatus for generating shock waves of the type mentioned, which may be manufactured simply and cost-effectively and which may be designed reliably concerning its application and more flexibly as regards its size.

BRIEF SUMMARY OF THE INVENTION

The underlying idea of the invention is to use piezoelectric fibers, hereinafter called piezofibers, for generating shock waves. The essential thought of the invention is that the piezofibers are integrated in a composite material. They are controlled with a control unit and together with said control unit they form the shock-wave generating part.

Piezofibers are known for the use in the aviation industry, especially for the use as impact sensors that may be integrated in the skin of an aircraft wing in conformity with the structure. They are used for the detection of small impact events such as a bird's impact.

For the generation of the shock waves the indirect piezoelectric effect of the fiber materials is used. An external electric field exerts opposite forces on the positively and negatively charged ions in the crystal lattice. This leads to a deformation of the fiber materials. The piezofibers stretch mainly in their lengthwise direction. This short stretch is used for generating shock waves in the apparatus according to the invention.

Preferably, the piezofibers are integrated in the composite material such that their lengthwise direction shows to the area to be treated and/or to the shock wave's direction of propagation. In this way a high energy density in the focus range may be achieved.

The piezofibers may be embedded in the composite material in a simple and uniformly distributed way. Thus, the connection of the piezofibers with the composite material is homogeneous.

The contacting of the piezofibers may be realized by a common electrically conductive layer according to the interconnection requirements. Hence, the complex interconnection of a multitude of piezoelectric ceramic elements of the known electro-acoustic transducers is no longer required.

The piezofibers integrated in the composite material form at least one module with the composite material.

This at least one module may form a special unit in a preferred embodiment of the apparatus according to the invention. However, it is also imaginable that the at least one module forms a unit by means of common electrically connected piezofibers.

Furthermore, the piezofibers may be put in curved structures. In both embodiments mentioned above the at least one module may be designed in geometrically different forms.

This facilitates a high flexibility in the embodiment of the shock-wave generating apparatus. Hence, apparatuses for generating shock waves of different geometric forms may be realized.

Additionally, several modules may be arranged next to one another. The modules may be interconnected individually, in groups or with one another.

In order to achieve a compact arrangement of the shock-wave generating apparatus, the at least one module is preferably arranged on a carrier.

The individual piezofibers may be designed in a commonly contacted way on the respective terminals in a separate embodiment. If the module carrier is designed in an electrically conductive way, one of the two contacts may be connected with the module carrier.

The module carrier may have different geometric forms.

The above mentioned preferred variation of the apparatus according to the invention for generating shock waves concerning the geometry allows for the possibility of a miniaturization of the apparatus. This enables the production of small-sized shock-wave generating apparatuses of the mentioned type for intracorporal applications.

Plane modules with piezofibers integrated in the composite material with any shaping may be manufactured.

Hence, for special applications not only smaller shock-wave generating apparatuses may be realized with the apparatus

according to the invention but also plane shock-wave generating apparatuses with different focus geometries.

BRIEF DESCRIPTION OF THE DRAWING

These and other features, aspects and advantages of the present invention will become better understood with reference to the following description, appended claims, and accompanying drawing, where:

Figure 1 shows a side and a front view of a preferred embodiment of the invention,

Figure 2 shows a side and a front view of a further embodiment of the invention and

Figure 3 shows front view of an embodiment of the invention with several modules arranged next to one another.

LIST OF REFERENCE NUMBERS

- 8 shock-wave generating apparatus
- 12 shock-wave generating part
- 14 piezofibers
- 16 composite material
- 18 medium suitable for the shock-wave transmission
- 20 coupling membrane
- 22 module
- 24 module carrier
- 26 direction of propagation of the shock waves
- 28 shock-wave focus
- 30 respective terminals
- 32 shock wave on a frontal area of the piezofibers

34 focus line

36 radiating surface of the module

5 38 module group

10 Equivalent parts are indicated by the same reference
numbers.

DETAILED DESCRIPTION OF THE INVENTION

The invention summarized above and defined by the enumerated claims may be better understood by referring to the following detailed description, which should be read in conjunction with the accompanying drawing. This detailed description of a particular preferred embodiment, set out below to enable one to practice the invention, is not intended to limit the enumerated claims, but to serve as a particular example thereof.

Figure 1 illustrates a shock-wave generating apparatus 8 showing a shock-wave generating part 12 and a medium 18 suitable for the shock-wave transmission which fills a volume between the shock-wave generating part 12 and a coupling membrane 20. As a medium 18 suitable for the shock-wave transmission water or a gel is used, for instance. The coupling membrane 20 serves the energetically low-loss coupling of the shock-wave generating apparatus 8 to a part of the body to be treated.

The shock waves are generated by the shock-wave generating part 12 and propagate in the illustrated direction 26.

Based on the given geometry of the shock-wave generating part 12 they are bundled in a shock-wave focus 28. The shock-wave focus 28 is the area with the highest energy density. In the embodiment illustrated in Figure 1 the shock-wave generating part 12 is designed in the form of a spherical segment. This leads to a focusing of the shock wave. Focusing may be realized in the known, thus not to be specified, electronic way.

The shock-wave generating part 12 consists of piezofibers 14 integrated in a composite material 16. The piezofibers 14 are electrically connected on the respective terminals 30 and high voltage is applied. High voltage is preferably applied in a pulse-shaped way.

The piezofibers 14 are integrated in the composite material 16 such that they preferably show to the direction of propagation of the shock waves 26 in their lengthwise

direction, since they mainly propagate in this direction and may thus reach the highest lift.

5 This short stretch of the piezofibers 14 is used for generating shock waves in the apparatus according to the invention. If a high-voltage pulse is applied to the piezofibers 14, the piezofibers 14 stretch triggering off a shock wave on a frontal area 32 of the piezofibers 14. The generated shock wave is bundled in a shock-wave focus 28
10 according to the geometry of the shock-wave generating part 12.

The composite material 16 forms a spatial unit, hereinafter called module, with the integrated fibers 14 in
15 the illustrated embodiment. The module 22 in the geometric form of a spherical segment is arranged on a carrier 24.

The piezofibers 14 are designed in a commonly contacted way on their respective terminals 30 and they are each
20 connected via incoming cables with a control device which is not illustrated herein.

In an especially preferred embodiment of the apparatus according to the invention the module 22 is arranged on an
25 electrically conductive module carrier 24 which is connected in an electrically conductive way with one of the two connections, not illustrated herein, of the terminals 30, commonly contacted each, of the piezofibers 14.

30 As already specified above the geometry of the shock-wave focus 28 may be determined by the shaping of the module carrier 24 and the module 22.

In the illustrated first embodiment in Figure 1 a shock-
35 wave focus is generated in the form of an ellipsoid.

In the illustrated second embodiment shown in Figure 2 a horizontal cylindrical focus line 34 is generated. For this, the shock-wave generating part 12 is designed geometrically in
40 the form of a pipe segment.

According to a preferred embodiment of the invention as illustrated in Figure 3, several modules may be arranged next to one another. The individual modules 22 may have different
45 sizes and different forms as regards their radiating surface

36. The modules 22 may be individually controlled. A mutually delayed control of the individual modules 22 may be achieved in this way, for instance. However, they may also be interconnected and controlled in module groups 38.

5 High voltage is applied in a known way by a high-voltage pulse generator the first pole of which is connected to one terminal 30 of the commonly contacted piezofibers 14 and the second pole of which is connected to the other terminal 30 of the commonly contacted piezofibers 14.

10

In a preferred embodiment the common terminal 30 of the piezofibers 14 on the module carrier 24 is connected with the preferably electrically conductive carrier material 24.

15 The module carrier 24 may thus be directly connected to a pole of the high-voltage pulse generator.